### Liquid Xenon for medical imaging and physics applications

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### Outline

Property of liquid Xenon **Given Stature:** Light-charge sharing Liquid Xenon for physics Liquid Xenon for Positron Emission Tomography Concept **Prototype Expected performances** 



## Key properties of noble liquids

	Z (A)	BP (Tb) at I atm [K]	liquid density at Tb [g/cc]	ionization [e-/MeV]	scintillation [photon/MeV]
He	2 (4)	4.2	0.13	39,000	22,000
Ne	10 (20)	27.1	1.21	46,000	30,000
Ar	18 (40)	87.3	I.40	42,000	40,000
Kr	36 (84)	119.8	2.41	49,000	25,000
Xe	54 (131)	165.0	3.06	64,000	68000*

LXe: high density, lots of charge and light

Zero electric field Some uncertainties

Infinite electric field

Gaitskell 2005



### Fabrice Retière Energy loss in noble liquid Scintillation, ionization and heat

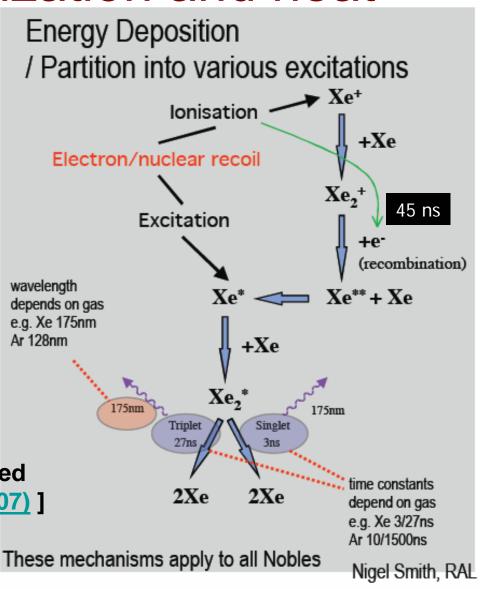
' light

phonon)

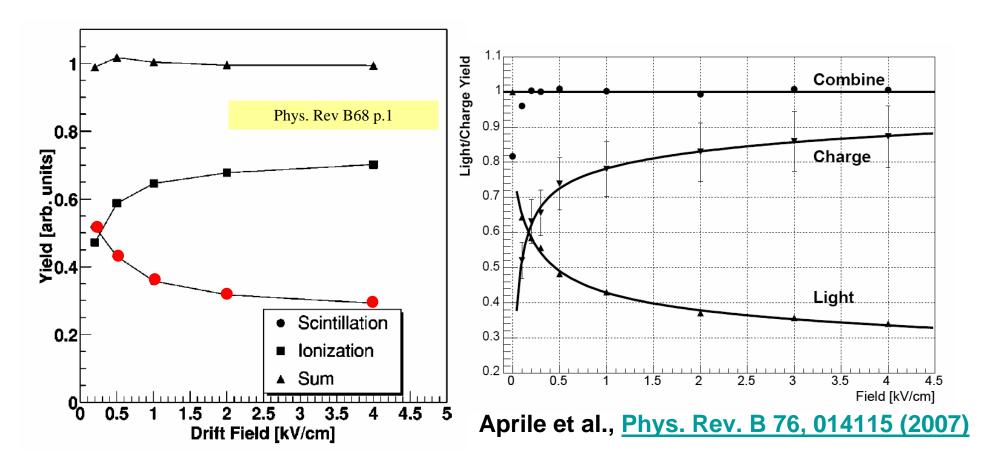
$R^* + R \rightarrow R_2^* \rightarrow 2R + hv$	Deep UV light
or	Ionization
$R^+ + R \rightarrow R_2^+,$	Heat (IR, phor
$R_2^+ + \underbrace{e^-}_{R^*} R^{**} + \\ R^{**} \rightarrow e^{-}$	- R, $R^* + heat$ $R^* + R \rightarrow R_2^* \rightarrow 2R$

Electron-ion recombinations enhance scintillation light Light and charge are anti-correlated

1 electron-ion lost  $\Rightarrow$ 1 UV photon produced [Aprile et al., Phys. Rev. B 76, 014115 (2007)]



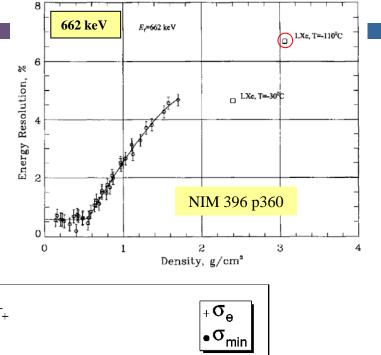
### Effect of electric field

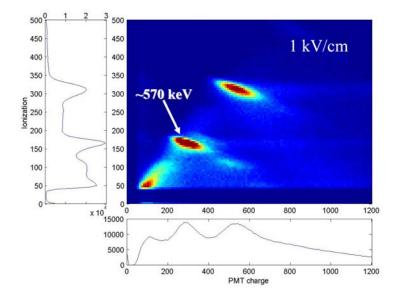


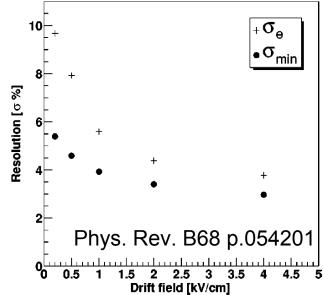
Note the discrepancy in charge fraction between papers Scintillation light is normalized differently.

### Event by event variation

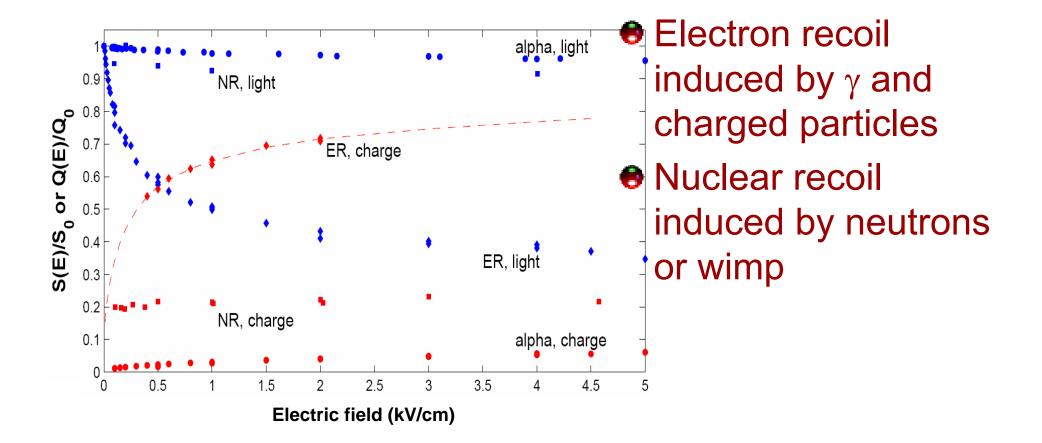
- Energy resolution from ionization much worse than Fano limit
  - Density fluctuations
    - Variation of recombination
  - Correlation with scintillation improves resolution







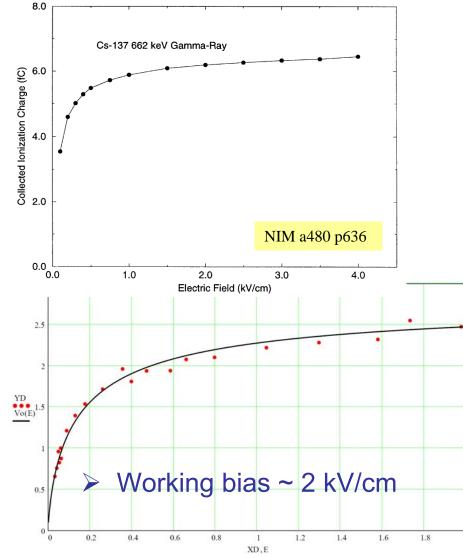




Aprile et al., Phys.Rev.Lett.97:081302(2006).



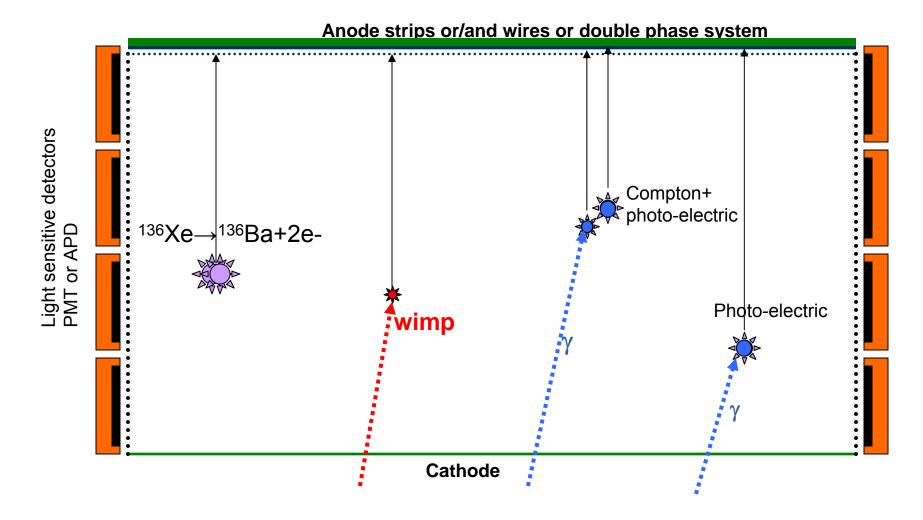
### **Measuring** ionization



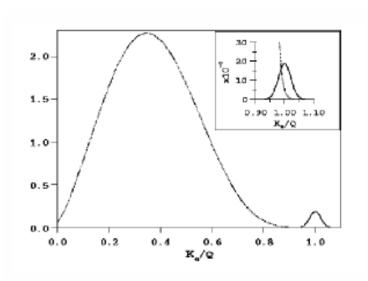
Ionization saturates to 15.6 eV/pair □ Recombination ~ 5% at 2kV/cm Electron lifetime □ With 1 ppb impurity = 1 ms Drift velocity □ 2.5mm/µs at 2kV/cm  $\succ$  100 µs for 25 cm drift Very small diffusion □ Primary electron range dominates About 1 mm at 511 keV

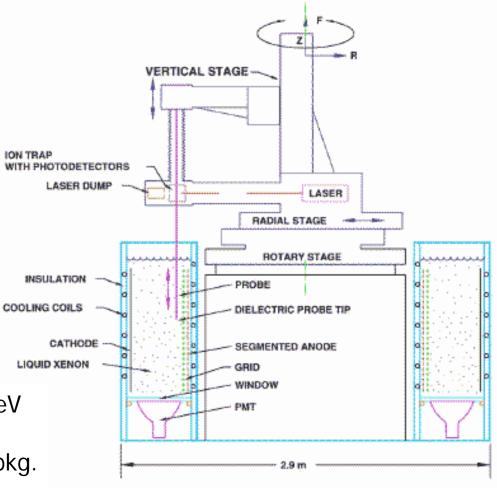


## 3D imaging in liquid Xenon

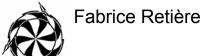




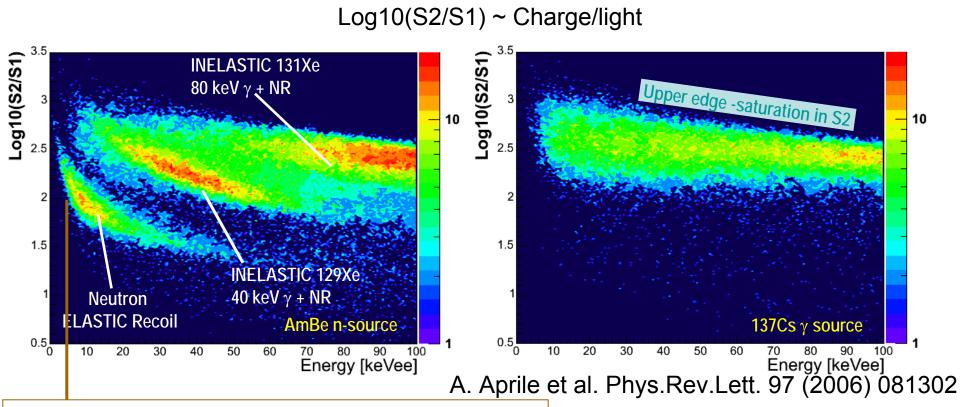




- LXe TPC for Energy Peak (2e) at 2.5 MeV
- Light and charge for energy resolution
- Ba<sup>+</sup> ion daughter extraction to reduce bkg.
- Aim for >10<sup>28</sup> years; 10 meV sensitivity



### Key to dark matter searches



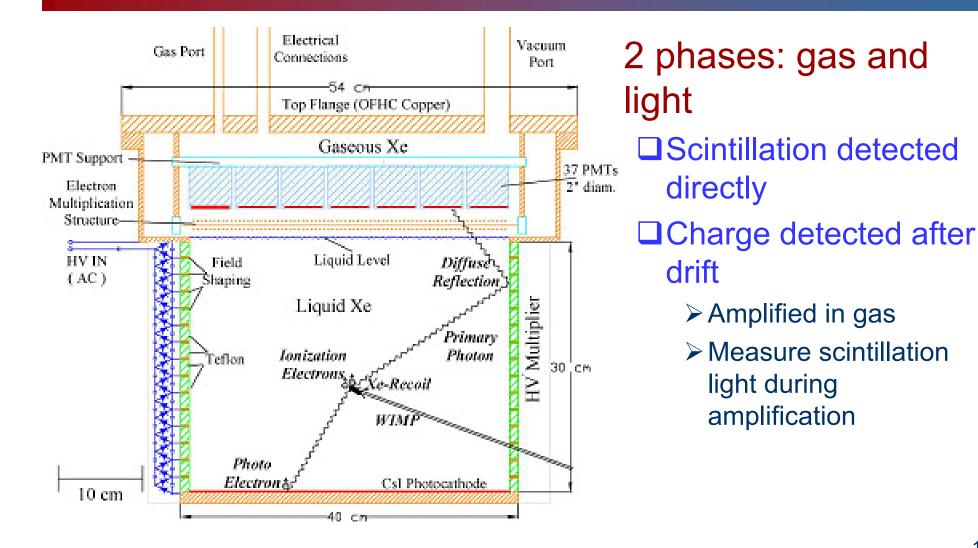
### 5 keVee energy threshold = 10 keV nuclear recoil



Key: fraction of light and charge depends on density of ionization
Lower charge/light ratio for nuclear recoil (WIMP)
Issue: small signal Q~500 e- (need very low noise or amplification)

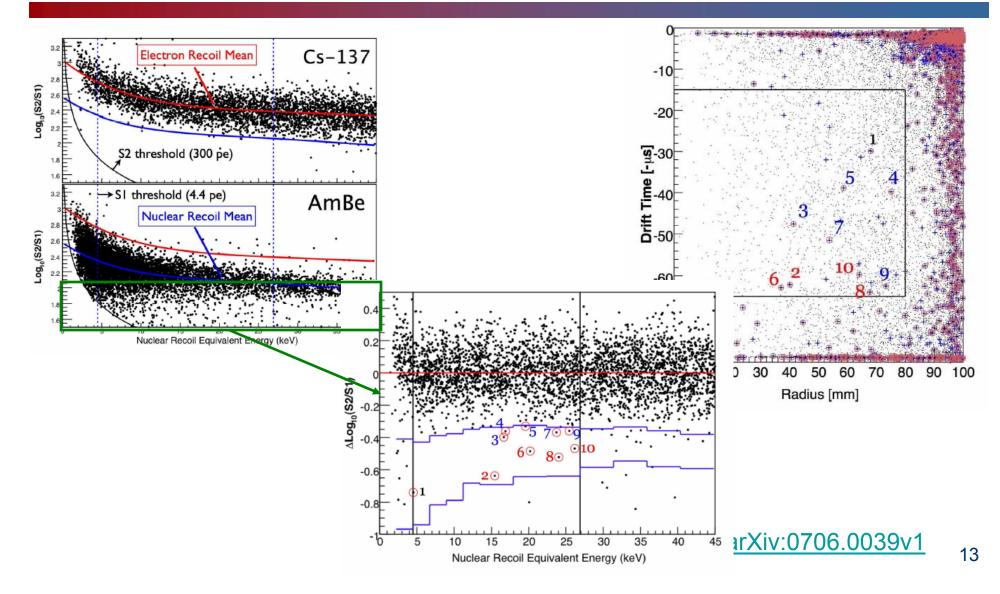


## **XENON 10 principle**



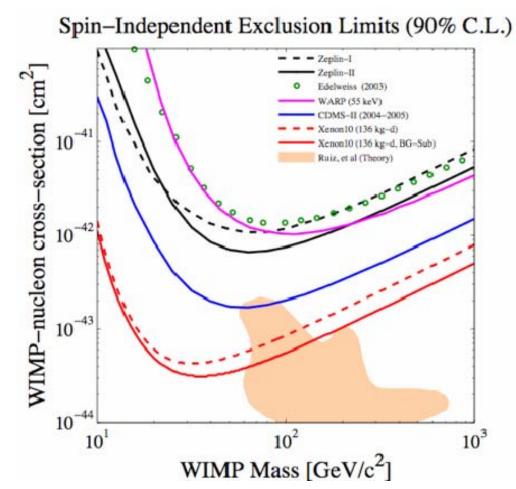


# Searching nuclear recoil candidates





# All events consistent with background



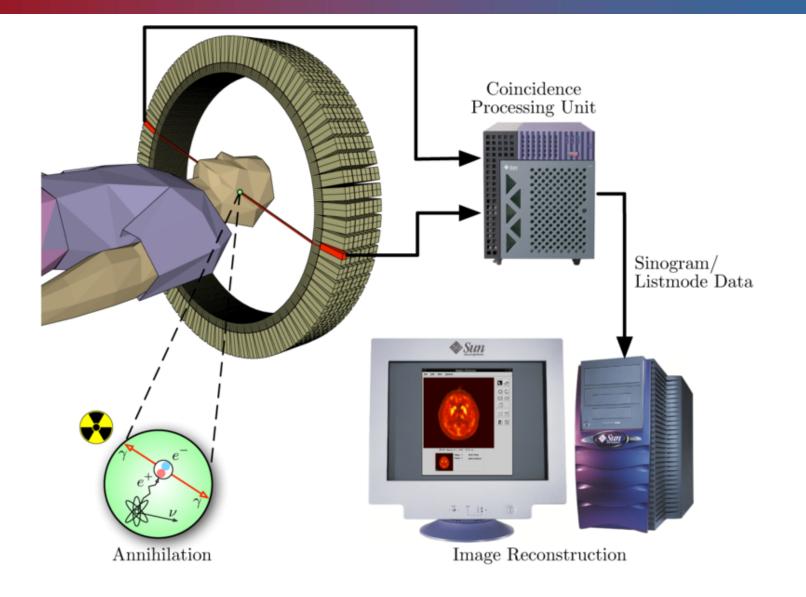
Very significant improvement over Germanium based detector Next step: bigger detector

## Liquid Xenon for Positron Emission Tomography

- Efficiency: 70-95%
- Position resolution < 1 mm</p>
  - □ Depth of interaction resolution ~1-5mm
- Two hit separation < 10 mm</p>
  Allow reconstructing consecutive Compton interactions
- Timing resolution 1ns or better
- Energy resolution 5% (FWHM) or better @ 511 keV
- High counting rate
- Low cost (no patent)



## **Positron Emission Tomography**



### Micro-PET

Research scanner
 For small animal
 Small diameter
 High resolution



Typical performance (LSO) □Efficiency: 85% Position resolution: 6 mm Depth of interaction issue Resolution at center of field of view < 1.3 mm□ Timing resolution: 3 ns (FWHM) □Energy resolution: <18% (FWHM) @ 511 keV



### Scintillation

Scintillator	BGO	LSO	LXe	Pros/cons
Density, g/cc	7.1	7.4	3.1	-
Yield, photons/keV	6.4	32	68 (EField=0)	+
Decay time, ns	300	40	2.2 (27, 45)	+
Wavelength, nm	480	420	178	-
Photo-fraction	42%	33%	22%	-

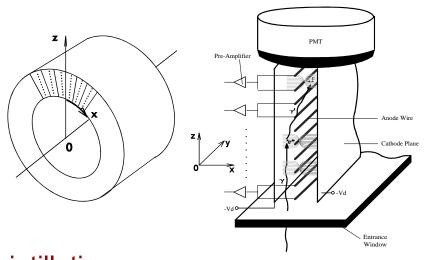
### Measure ionization as well: more quanta

□ Full collection of electron with electric field
 ▷ Slow drift, no improvement in timing
 □ Greatly Improve position and energy resolution

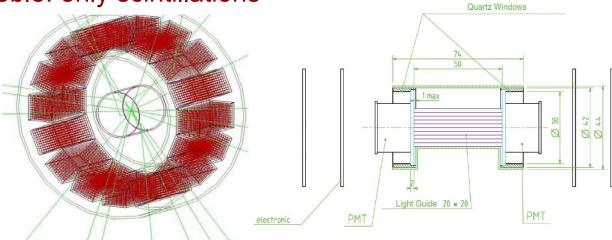


### Fabrice Retière Sample of LXe PET being developed

### □ LIP: scintillations and ionizations



Grenoble: only scintillations

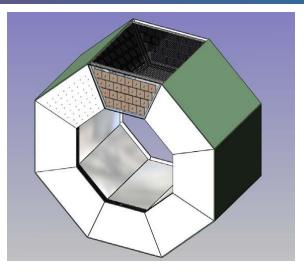


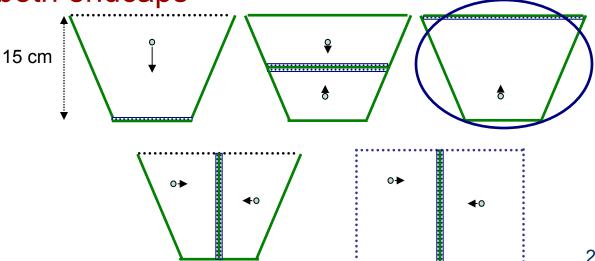
## **Our solution**

- - Define a region of interest in the drift volume
  - Reduce pile-up by matching with ionization cluster position
    Provide timing resolution

## **Detector geometry**

- Number of sectors
  - **3**,10, 12
    - > 12 optimum for pile-up rejection
- Electron drift
  - Radial, axial, azimuthal
    - Radial towards outer radius
- Light sensors cover both endcaps

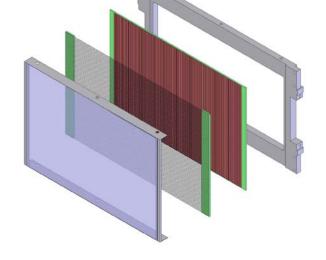






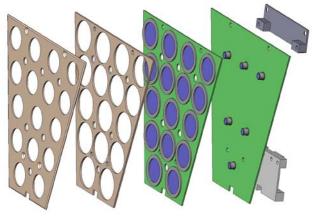
### □ 12 sectors.

- Field cage formed with strips (between sectors) and wires (ends)
- Cathode: resistive kapton on ceramic plates



### Anode module

- 96 wires, 96 strips
- SS and kapton PCBs
- AC decoupling with kapton?



### □ APD module

- 16 APDs and 6 LEDs for monitoring
- 1 HV line and 16 LV lines (HV tuning)



## Light detection with APD

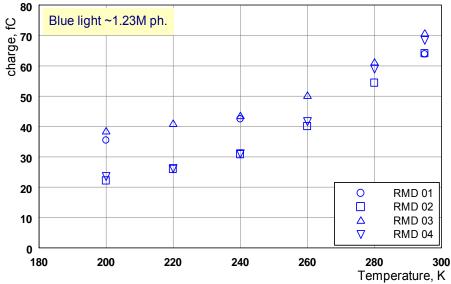
### PMT

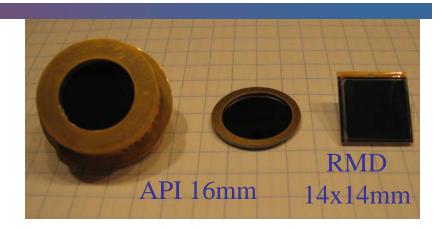
Low QE not compact

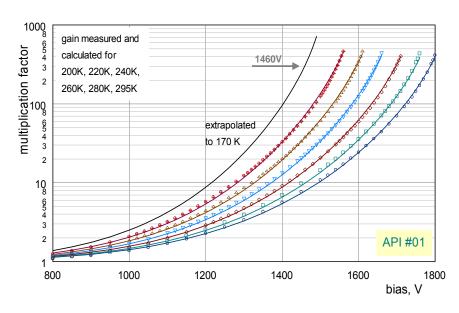
APD

- Generation Work at low T
- □ QE~0.5-100% for UV light
- Fast
- Large area from API and RMD

But RMD QE drops with T







### **Custom electronics**

### Light detection

 □ Fast and low noise for Cd = 200 pF
 > Signal ~ 20,000 electrons
 □ BJT gives 4000 e- ENC for 20 ns peaking time
 □ 16 channels



### Ionization signal

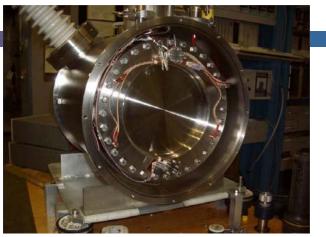
- Low noise, rather slow for Cd = 30 pF
   JFET gives 600 e-ENC for 270 ns shaping time
- □ 32 channels

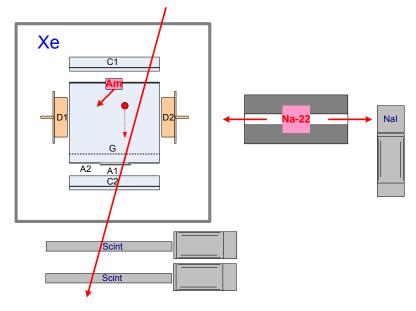


## Small scale prototype

- Run May-August 2006
  - □8.5 I cryostat
  - □ 3x3x3 cm<sup>3</sup> TPC
    - ≥ 2 anodes
    - ➤ 1 grid (active)
    - ➢ Readout with 20 MHz digitizer
  - **2** 16 mm APD
    - ➢ Readout with 1 GHz digitizer
- Main measurements

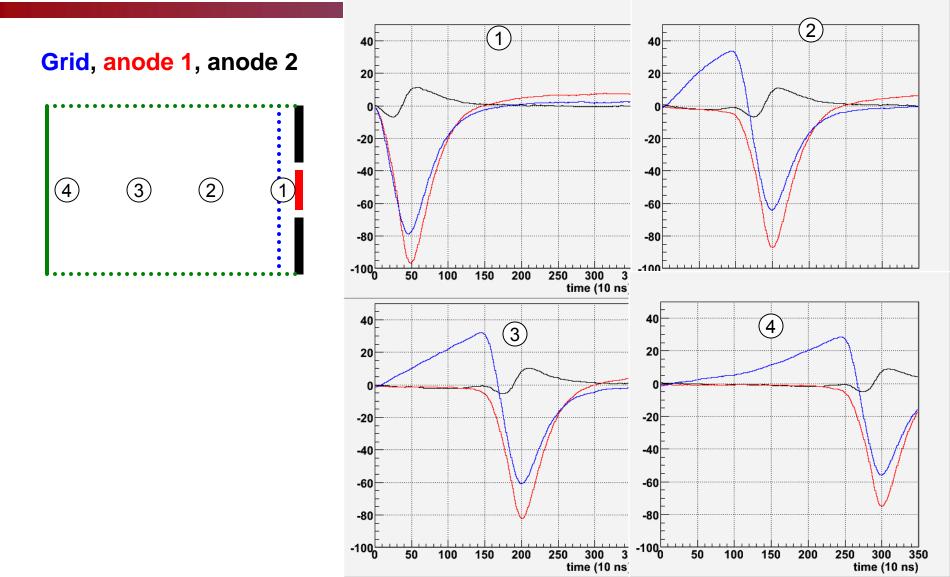
  - □Na22 source of 511 keV
- Good electron lifetime achieved



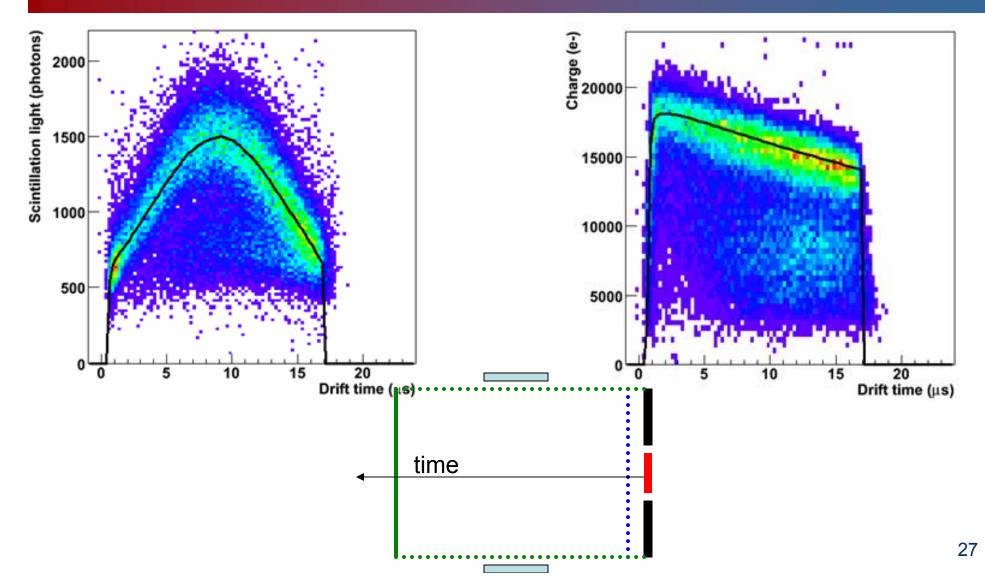




### Understanding current Work like an ionization chamber

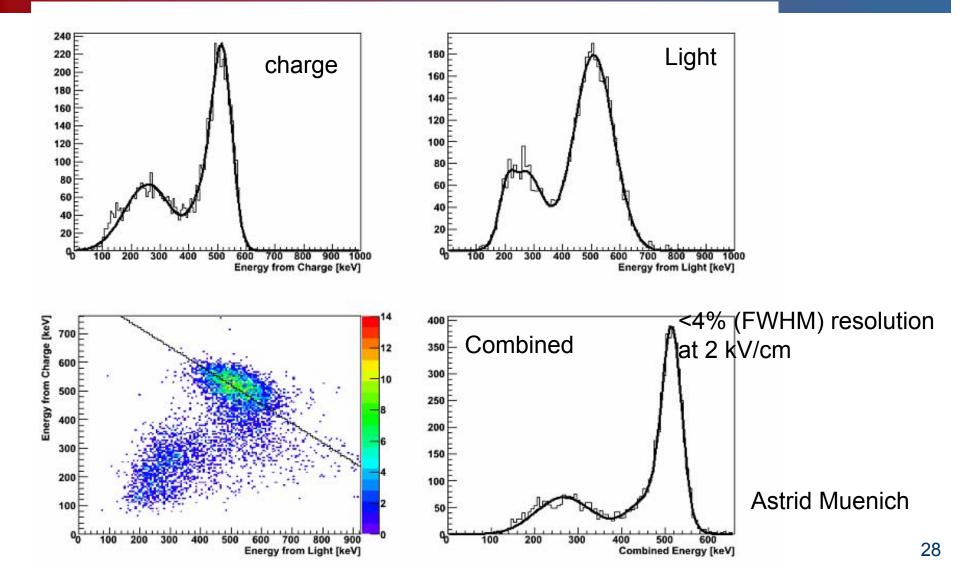








Fabrice Retière Combining light and charge for optimum resolution





### Achievements:

 $\Box$  200  $\mu$ s electron lifetime

Need to demonstrate scalability to next prototype

□1 ns timing resolution

□4% (FWHM) energy resolution

Issues

□ No absolute light calibration

After canceling light/charge fluctuations, resolution dominated by APD noise and solid angle fluctuations (light-position correlation)



# Estimating the micro-PET performance by simulations

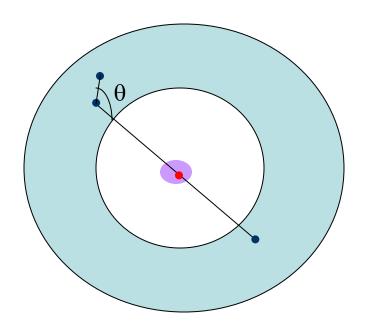
- Geant 4 for photon interactions
- Parameterize detector response
  - Energy, timing and position resolution
  - □ Hit merging
  - □ Efficiency (effective)
- Calculate count rates from the probabilities of detecting 0, 1 and 2 photons per annihilations

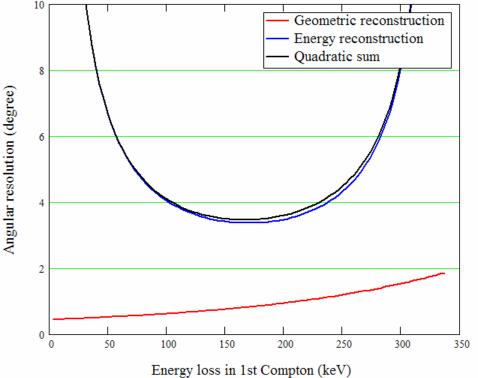
- Develop an algorithm for reconstructing Compton interaction sequence
  - Crucial to find the first interaction point
    - Choosing the wrong point worsen resolution
  - Useful to reject background



## 511 keV photon interaction Using Compton information

- Probability of interaction fo 511 keV
  - □ 3.6 cm attenuation length
  - □ 30% photo-electric
  - □ 70% Compton

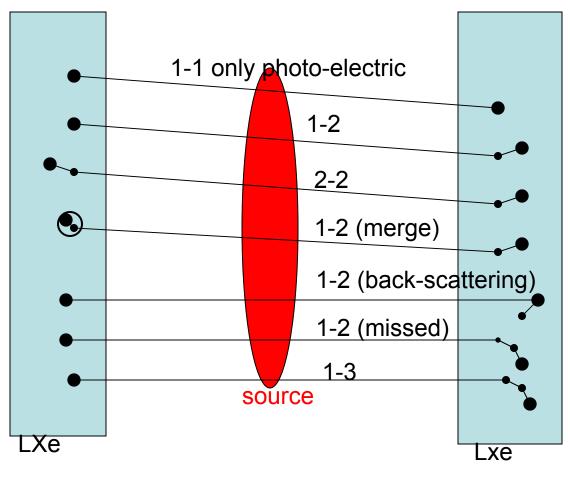




$$\theta = \cos^{-1}(1 - me \cdot \frac{Eloss - Ei}{Eloss \cdot Ei})$$



## Many different Compton configurations



- Crucial to select right first point
- Minimum energy threshold per point is 50 keV
- Some points merge
   Merging recover some low energy points
- Backscattering significant



## Reducing the background

- Background sources □ Scatter in patient Lower energy photon Wrong geometrical Compton angle Random: 2 photons from 2 different annihilations Uncorrelated line of response  $\succ$  Often, one of the photons undergoes a scatter before reaching the
- Scatter Fraction 0.3 0.3 Current micro-PET (Focus 120) **Scattering Fraction** 0.25 0.2 250keV threshold 0.15 350keV threshold 450keV threshold 0.1  $\Delta X=1 \text{ mm}. \Delta E/E=9\%$ 10<sup>-1</sup> 1 10  $\gamma^2$  cut Compton criteria

UBC student Philip Lu

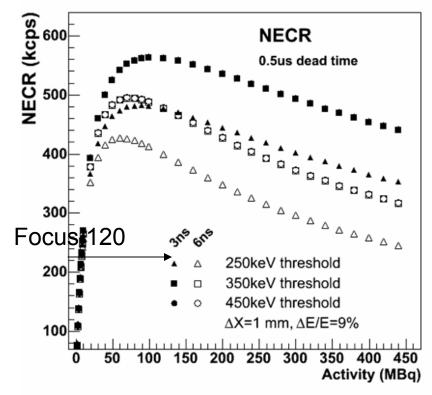
detector



## Optimizing the count rate

No Compton χ<sup>2</sup> cut is best for maximizing counting rate
 Reduce true much compare to background rejection
 Dead time in this calculation = 500 ns
 Very tough to achieve

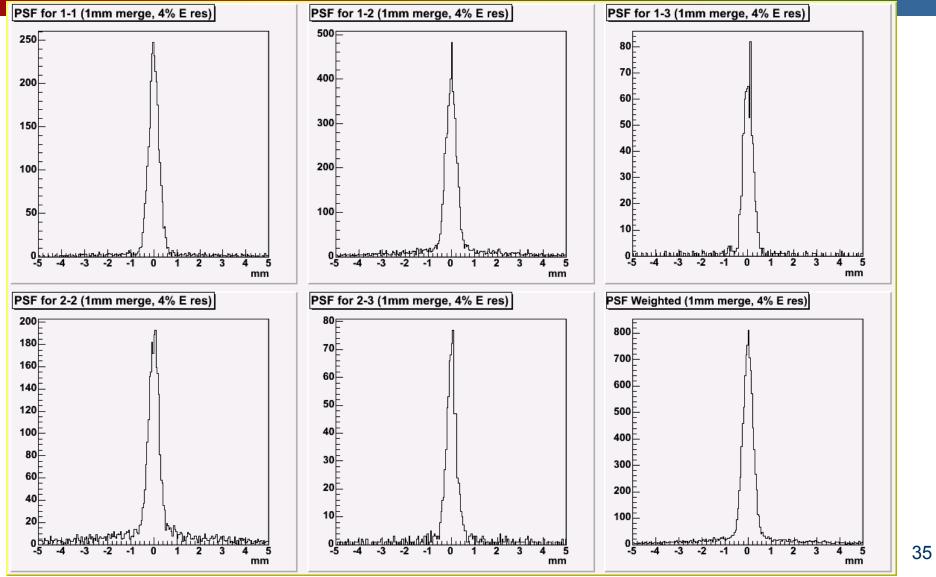
 $NECR = \frac{True^2}{True + Scatter + Random}$ 



Rat size phantom

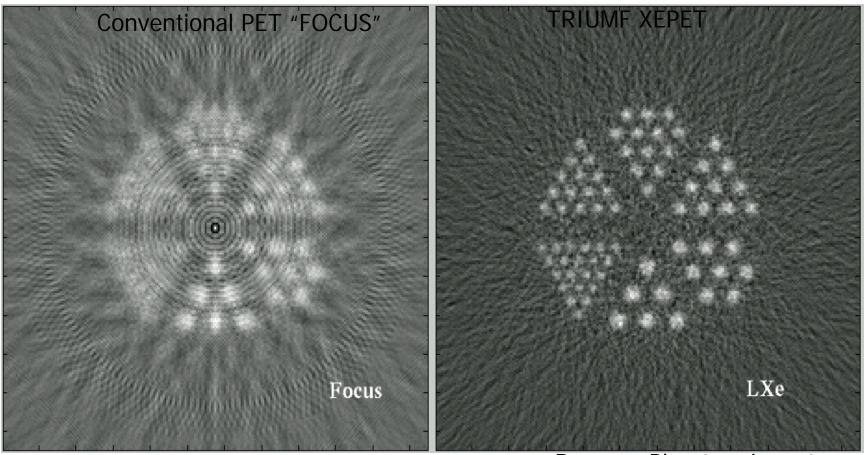
UBC student Philip Lu







Fabrice Retière Comparison of PET Image Simulations



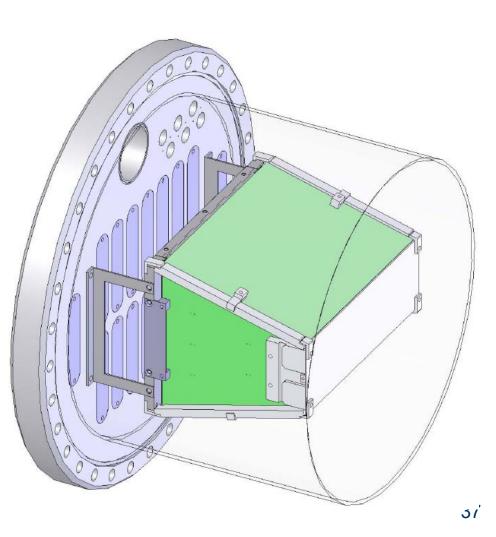
UBC student Philip Lu

Derenzo Phantom in water: 1mm dia. Minimum feature size.



## Continuing R&D program for PET

- End of 2007-2008 sector prototypes
  - □ Fits in existing cryostat
  - □ 96 anode strips, 96 grid wires
  - □ 32 APDs in ends
- Applied to CHRP for 2 sector prototype in 2008-2009
  - $\square \ \mu PET \ cryostat$
  - □ Final sector design
  - □ Final electronics and readout
  - Develop trigger
- 2010(?) μPET prototype
  - □ Fully (half) populated
  - Computing
    - data farm
    - Develop onlin reconstruction
    - Image reconstruction



## Summary

- Liquid Xenon is very promising for PET
  - □ Short attenuation length
  - Superior energy and position resolution
  - Compton reconstruction

### And for physics

- Double beta decay
- Dark matter search
  - XENON10 leading the pack

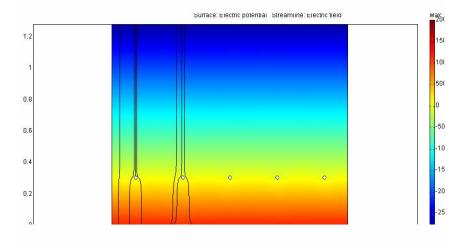
- Challenges ahead for TRIUMF LXe PET
  - Achieving ppb purity with lots of material
  - Designing custom electronics is necessary
    - Low noise, especially for APD
    - Triggering electronics
    - Minimize dead time
  - Data analysis must allow rapid diagnostic
    - Online processing
    - Rather complicated analysis

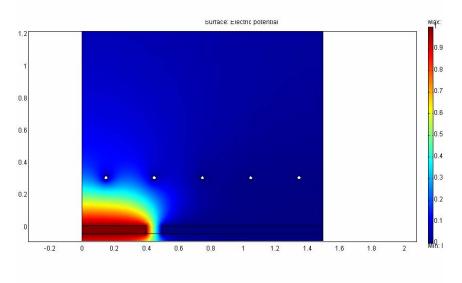
This work is supported by CFI-UBC-BCKDF and TRIUMF Tech Transfer Division and Science Division

### Back-up









- Drift field

   Electron trajectory

   Weighting field

   Induced current
  - ➢ Ramo theoem
- Preamp-shaper response function

