

Design and Performance of Liquid Xenon Detectors for PET

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- 1 PET and LXe**
 - PET: Positron Emission Tomography
 - Why use LXe for PET?
- 2 Proof of Principle**
 - Small Prototype
 - Data Analysis
- 3 LXe for Micro-PET**
- 4 Future: Design of full Micro-PET Ring**

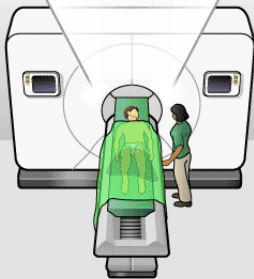
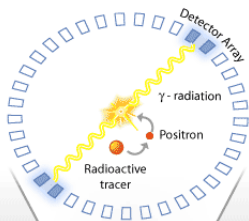
Working principle of PET

Principle

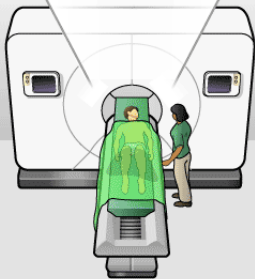
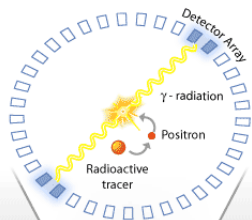
- Short lived isotopes decays emitting e^+
- e^+ drift range ≈ 1 mm (FWHM)
- e^+ annihilates into pair of 511 keV γ s
- Angle between γ s $\approx 180^\circ$
- Reconstruct line of response (LOR)
- Functional image (tumor screening)

Current Detector

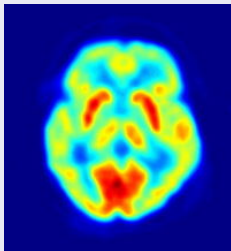
- Scintillating crystals in ring geometry
- Crystal provides discrete location \rightarrow No information about depth of interaction
- Energy resolution $\approx 18\%$ (FWHM)



Working principle of PET



Functional Image



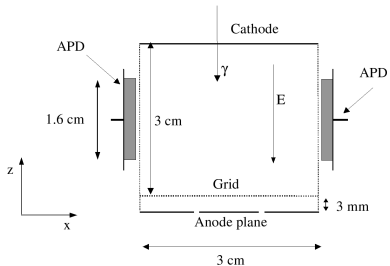
Current Detector

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Advantages of LXe for PET

- Attenuation length: 36 mm (at 165 K) → compact detector
- Produces ionization and scintillation light
→ combining both improves energy resolution:
energy resolution < 10 (FWHM)%
- Compton reconstruction
→ **3D localization** of first interaction (no parallax error, suppression of random and scatter backgrounds)
- Uniform **3D spatial resolution** throughout the field of view:
 < 1 mm in 3D
- **Timing resolution**: < 1 ns
- Cover **large volumes** with just one electrode array
→ high **sensitivity**
→ **Efficiency** $> 70\%$
- **Inexpensive** ($< \$ 3/\text{cc}$)

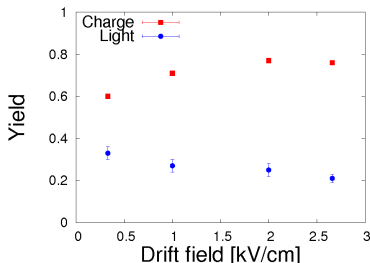
Time Projection Chamber (TPC)



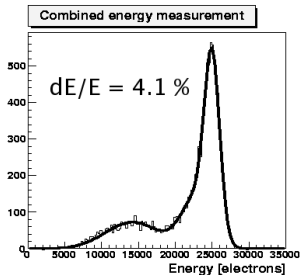
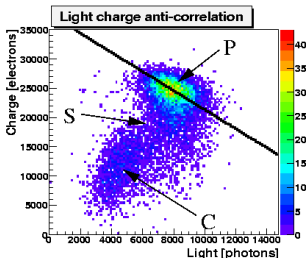
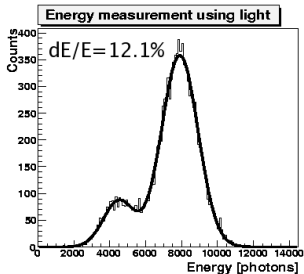
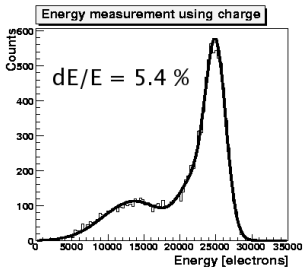
- TPC volume $3 \times 3 \times 3 \text{ cm}^3$
- $E = 1 \text{ kV/cm}$, $v_d = 2 \text{ mm}/\mu\text{s}$
- 2 APDs; solid angle $\approx 12\%$
- $511 \text{ keV } \gamma\text{s}$ from ^{22}Na

Achievements:

- Measured charge and light
- Studied energy resolution
- Understood detector contribution and limitations



Charge-Light-Anti-correlation



Understanding Error Contributions

Identify error contributions to energy resolution to quantify intrinsic resolution capability:

Charge

Electronics noise (3.5%)

Light

Electronics noise (4.7%)

Gain fluctuations (0.6%)

Solid angle fluctuations (5.6%)

Energy resolutions:

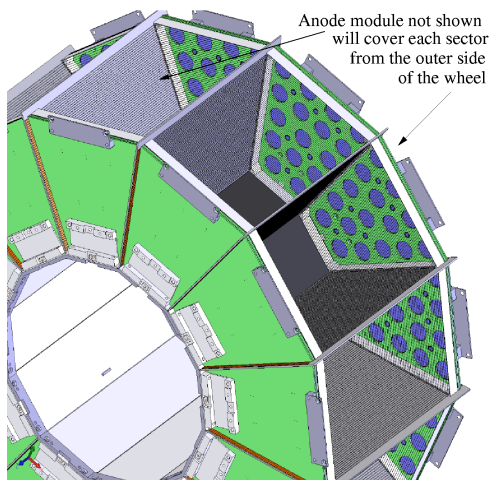
	meas. [%]	intr. [%]
Q	12.1	5.5
L	5.4	4.2
C	4.1	2.5

With position information available from charge, expect:

→ Light resolution: 10.4%

→ Combined energy resolution: 3.6% (< 8% FWHM)

Micro-PET Design

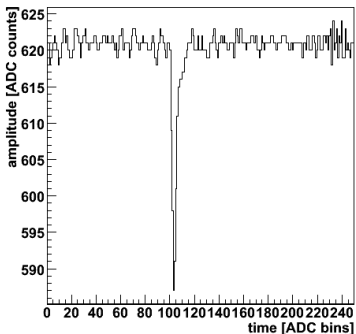


- 12 sectors, 32 APDs per sector, 96 anode wires, 96 anode induction wires
- Radial depth 12 cm
- Minimal dead space between sectors to increase active volume

Prototype Status

Finished test with 16 APDs

- 1st use of liquid purification
- Observed low signal amplitude



Probable Causes

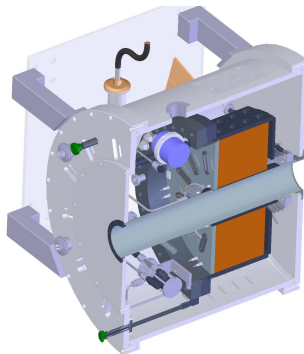
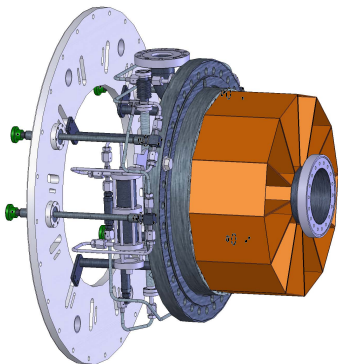
Impurities in LXe like H_2O
→ Attenuation too high

Possible Solution

Use gas **and** liquid phase purifier + longer high temperature bake-out

Outlook

CHRP Project: Design of cryostat in progress:

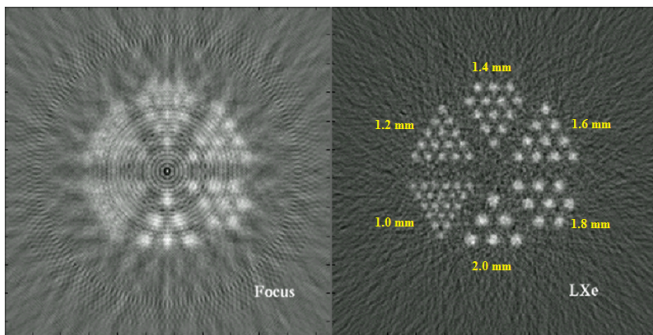


Build two new opposing sectors and operate in coincidence

BACKUP

Image Reconstruction from Simulations

Same simple reconstruction method (Filter-Back Projection) used for both (emphasis on resolution not image quality):



In the simulation, the limitations of the LXe system are primarily due to physics effects such as the positron range.

Position Reconstruction from Fast Light Signal

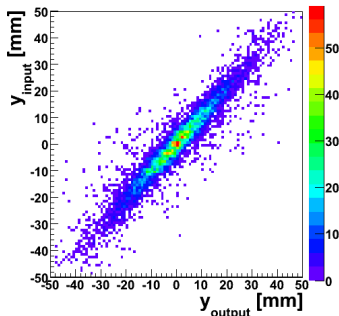
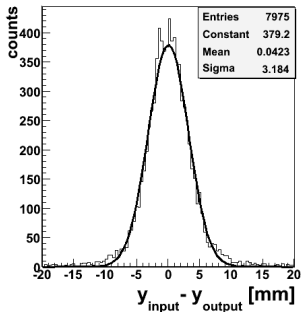
→ Important for high rate operation

Challenge

Input: 32 APD signals
Looking for 3D position

Solution

Neural Network
Implemented in ROOT/C++



Volume in which interaction can be found can be restricted to
 ~ 1 ml depending on noise.

Schedule

Activity	Start	End
Install and test single sector	2009-07	2009-11
Cryostat Design	2008-10	2009-09
Cryostat Construction	2009-06	2009-12
Cryostat Assembly	2009-10	2010-09
Sector Design	2009-01	2009-12
Sector Construction	2009-06	2010-06
Sector Assembly	2010-06	2010-09
Electronics Design	2009-06	2010-03
Data Acquisition System	2010-03	2010-12
Initial operation of multiple sectors	2010-09	2010-12
LXe coincidence meas. (point source)	2011-01	2011-06
LXe coincidence PET meas. (phantoms)	2011-06	2011-09
PET coincidence meas. (at UBC Hospital)	2011-09	2011-12