



# Liquid Xenon Detector for Medical Imaging

- Xe properties
- Ionization in Xe
- Scintillations
- Scintillators comparison
- Energy resolution
- Xe detectors in physics
- Micro-PET scanners

- Small TPC Tests
- R&D program
- Summary

- LXe detector for PET
- Detector geometry
- Light detection: APDs
- Light detection: electronics
- Charge measurements
- Electronics for ionization signals
- Full-scale prototype



## Xe Properties

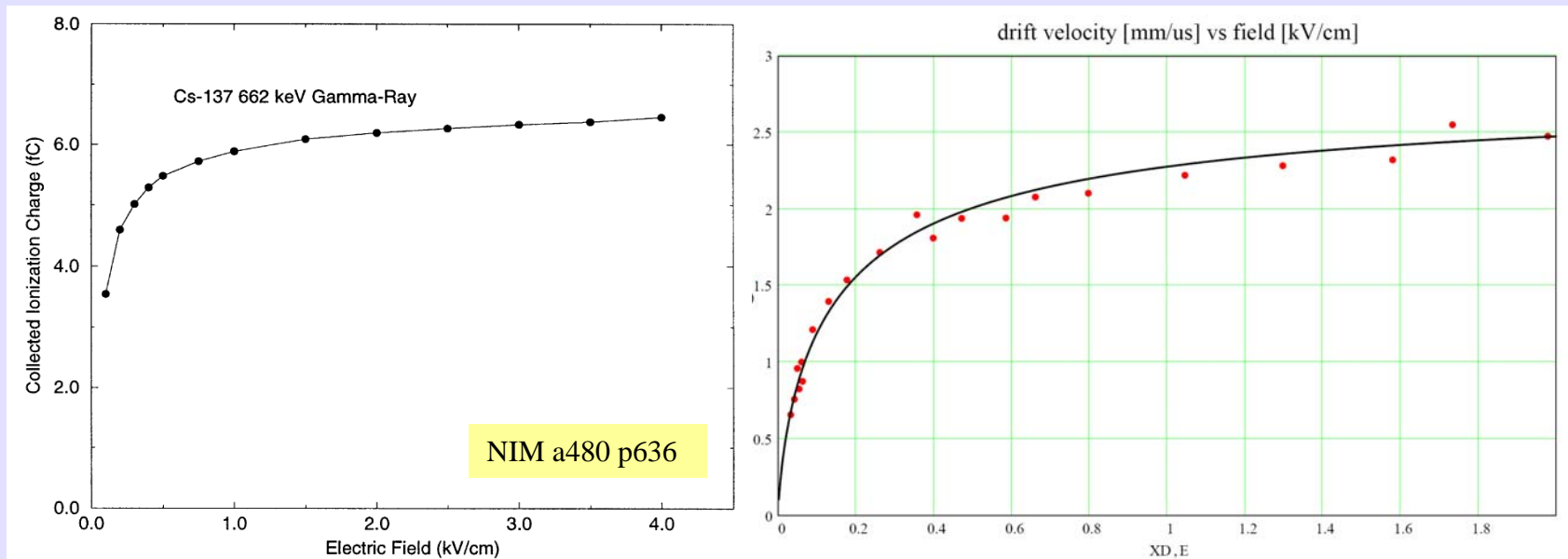
- $Z=54$ ,  $A=131.3$ . Isotopes: 8 stable and 2 unstable. Main: 129, 131, 132
- Boiling point 165.1 K, melting point 161.4 K. Density of liquid  $\sim 3.1$  g/cc
- Ratio liquid/gas 518
- Dielectric constant ( $f=0$ ) 1.96. Refractive index (VUV) 1.57-1.75
- Breakdown voltage  $\sim 1000$  kV/cm (???)
- Ionization potential 9.2 eV, Ionization yield  $W_i = 15.6$  eV (next slides)
- Radiation length 2.9 cm
- Scintillation energy 7 eV (178 nm), yield  $W_s=14.6$  eV (next slides)

Cost  $\sim 3$ \$/cc (liquid equivalent)



## Ionization in Xe

- ❑ Asymptotic high-E yield:  $15.6 \text{ eV/pair} \rightarrow 32.8 \text{ kel}$  for 511 keV
- ❑ Primary recombination at 2 kV/cm:  $\sim 5\%$
- ❑ Drift at 2 kV/cm:  $2.5 \text{ mm}/\mu\text{s}$  or  $4 \mu\text{s}/\text{cm}$ . Diffusion  $\sim 2 \text{ cm}^2/\text{s} \rightarrow 1 \mu\text{s}$  drift gives diffusion of  $\sim 14 \mu\text{m}$
- ❑ Purity: with  $1 \text{ ppb} \rightarrow e$  lifetime  $\sim 1 \text{ ms}$

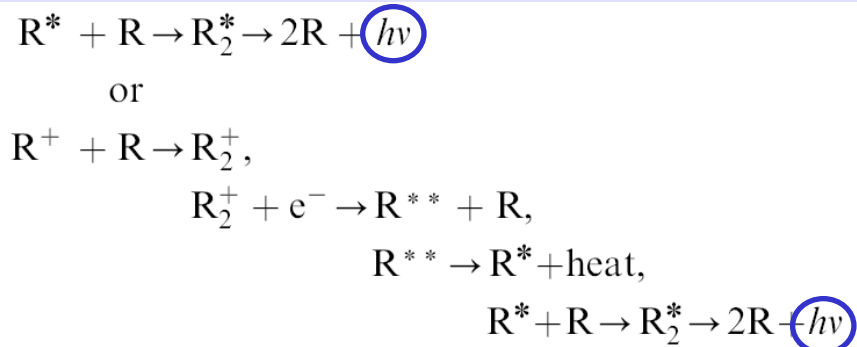


➤ Working bias  $\sim 2 \text{ kV/cm}$

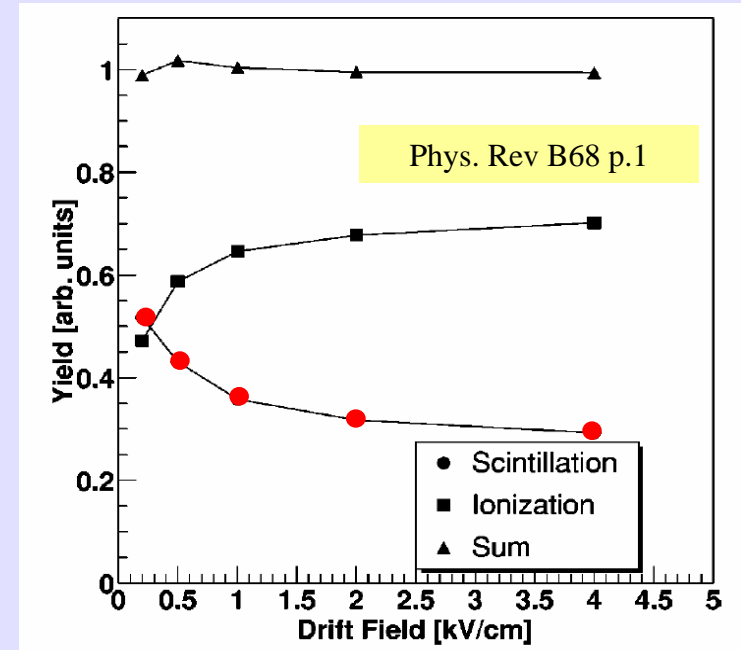


# Scintillations

- Two mechanisms: primary excitation and recombination



- Scintillation yield depends on HV



- VUV:  $\lambda = 175\text{-}178\text{ nm}$ ;  $W=14.6\text{ eV/ph}$
- Timing of excitation:  $\tau_1=2.2\text{ ns}$ ;  $\tau_2=27\text{ ns}$ ,  $\tau_3=45\text{ ns}$
- Attenuation length = 26-36 cm (absorption or Rayleigh?)
- IR:  $\lambda = 1\text{-}1.6\text{ mm}$ .  $W\sim 48\text{ eV/ph}$



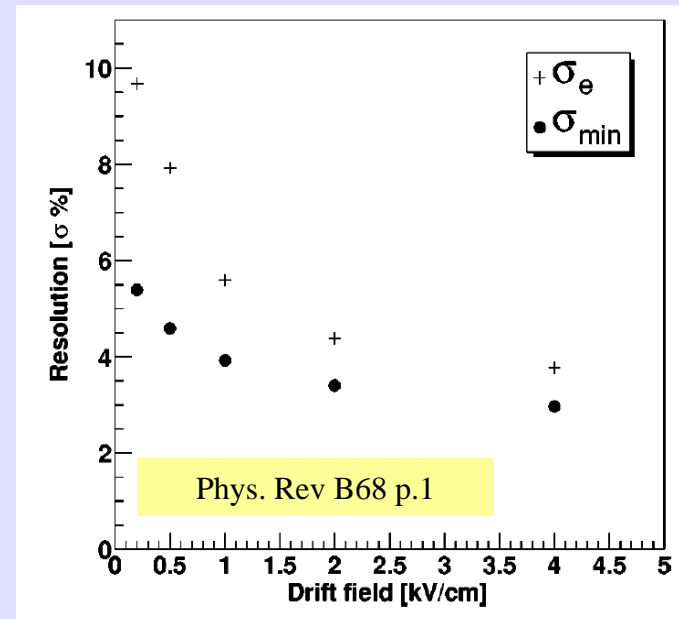
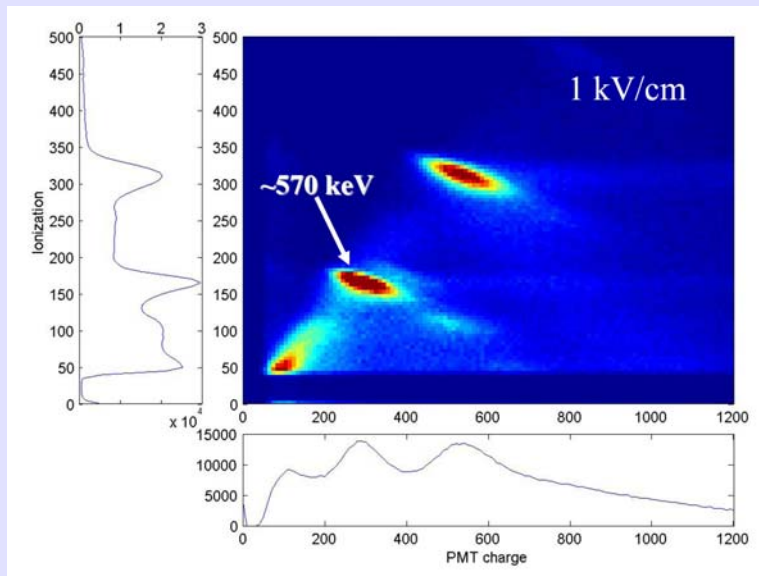
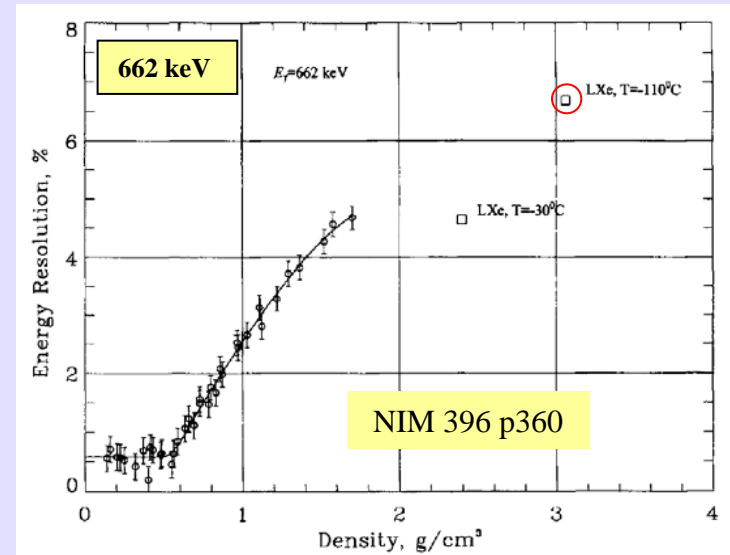
## Comparison with Other Scintillations

Scintillator	BGO	LSO	LXe
Density, g/cc	7.1	7.4	3.1
Yield, photons/keV	6.4	32	68 (20)
Decay time, ns	300	40	2.2/27
Wavelength, nm	480	420	178
Photo-fraction	42%	33%	22%



# Energy Resolution

- ❑ Ionization: much worse than Fano limit.  
 $F = 0.2 \rightarrow \text{fwhm} = 0.51\%$  for 662 keV
- ❑ No simple theory. Density fluctuations?
- ❑ Light: PE statistics. For 511 keV and  $\text{QE} \cdot \text{SA} = 5\%$ ,  $\Delta E = 4.4\%$
- ❑ Correlations improve E-resolution





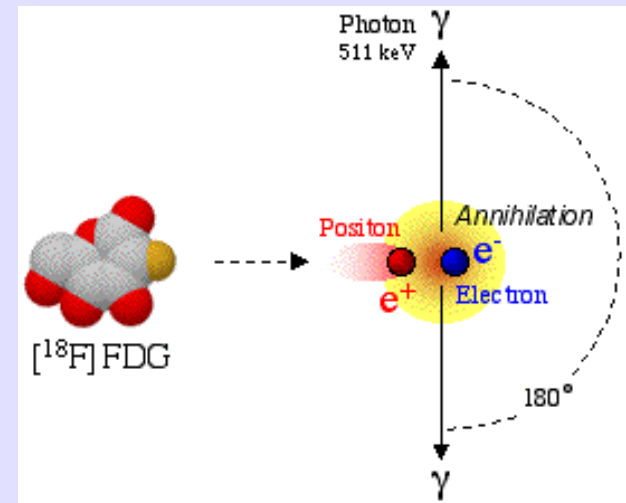
## Xe Detectors in Experimental Physics

- ❑ Dark matter:  
DAMA (Italy), XENON (Nevis), ZEPLIN
- ❑ Double- $\beta$  decay:  
EXO (Stanford)
- ❑ Astronomy:  
GRIT, XENA (Nevis-Lab)
- ❑ Nuclear physics:  
RD14 (CERN), MEG (PSI), RAPID (Italy)
- ❑ Medical imaging:  
LPSC (Grenoble), LIP (Portugal)



## PET Scanners

- ❑ A short lived isotope decays by emitting  $e^+$  which annihilates producing a pair of  $\gamma$  511keV. The scanner uses events to map the density of the isotope in the body
- ❑ Conventional scanners are based on inorganic scintillators (LSO)
- ❑ Micro-PET – small animal camera



### Typical performance

- ✓ Detection efficiency 85%
- ✓ Time resolution 3 ns (fwhm)
- ✓ Spatial resolution 6 mm
- ✓ Energy resolution 22% (@511 keV)
- ✓ No DOI information



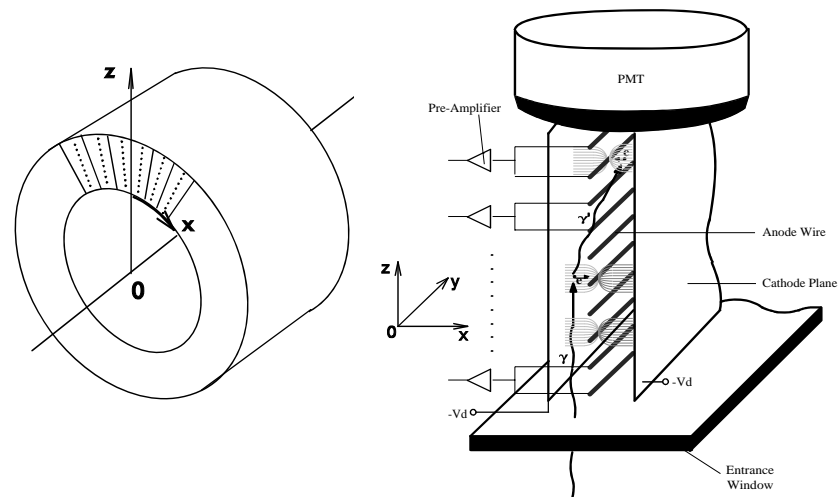


## LXe Detector for PET

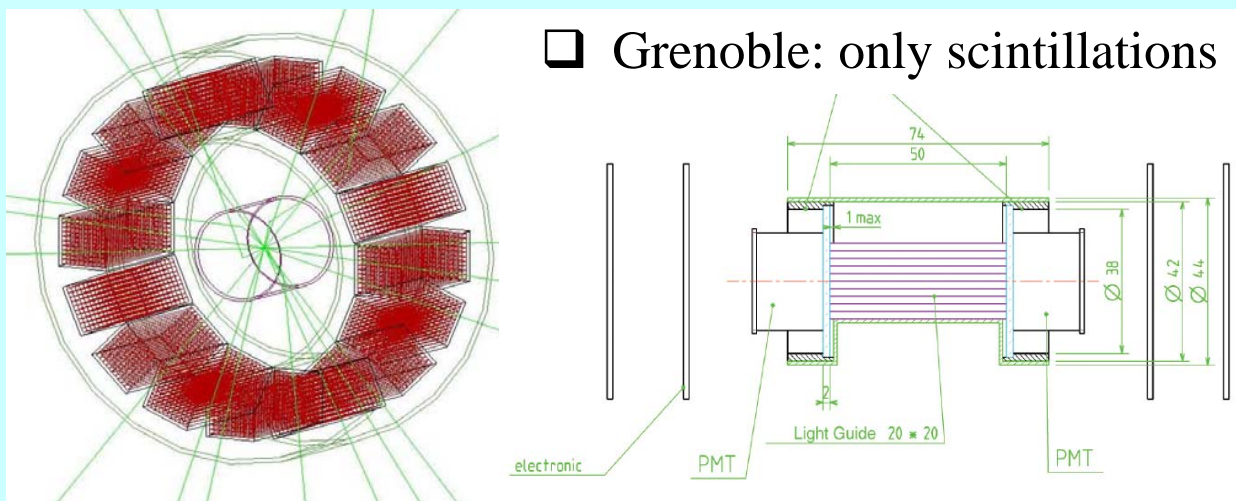
### Requirements (NIM A353 p189 )

- ❑ High spatial resolution along axial and trans-axial directions ( $\sim 1$  mm)
- ❑ Depth of interaction  $\sim 5$  mm
- ❑ Good time resolution ( $\sim 1$  ns)
- ❑ Energy resolution ( $< 20\%$ )
- ❑ High detection efficiency ( $> 70\%$ )
- ❑ High counting rate ( $> 10^5$  /s $\cdot$ cm $^2$ )
- ❑ Low cost

### ❑ LIP: scintillations and ionizations



### ❑ Grenoble: only scintillations





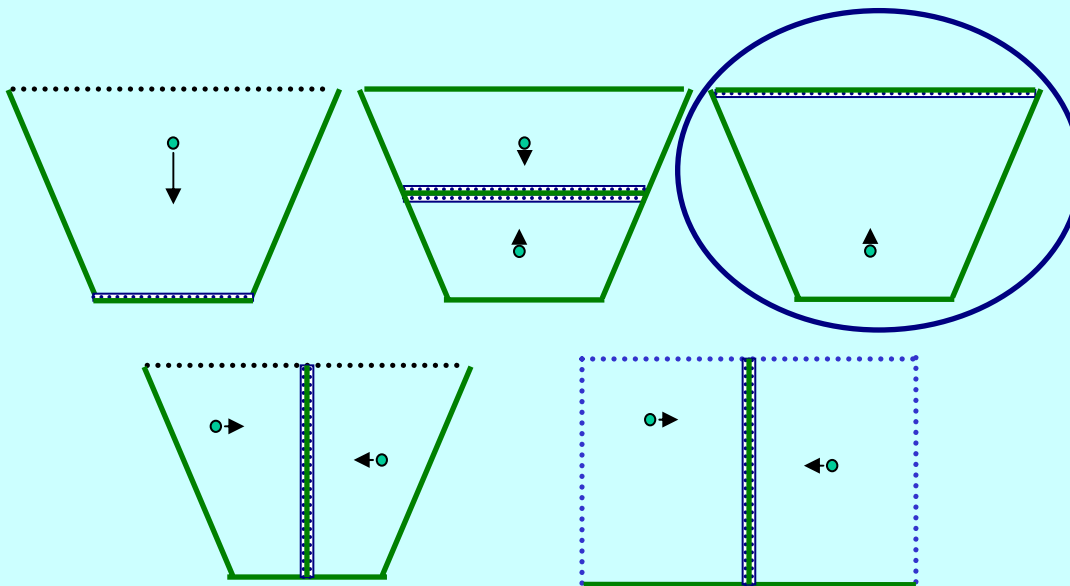
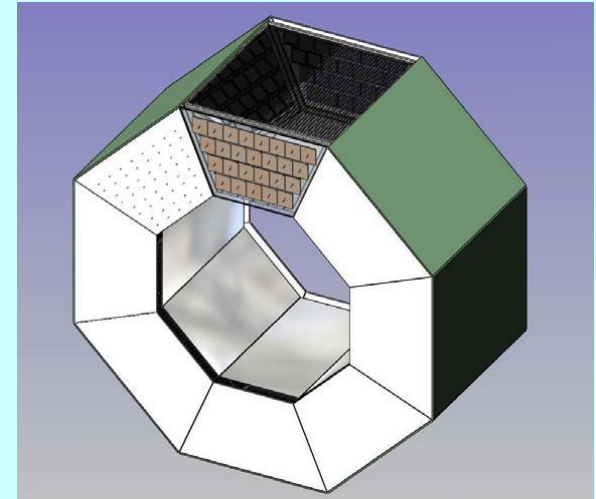
## LXe Detector for PET: Our Solution

- ❑ Use both scintillation light and ionization signals for energy reconstruction
- ❑ Trigger from scintillations
- ❑ Predict region of interaction from light (to minimize pileup and readout channels)
- ❑ Reconstruct one of coordinates from drift time (less channels)
- ❑ Other two coordinates with anode electrodes (strips with perpendicular orientation or strip and wires)
- ❑ Minimize induction gap (fast induced signals)
- ❑ Digitize shapes to get better timing and reject pileup



## Detector Geometry

- ❑ Sectors (8, 12, 16). Calculations of pileup conditions show that 12 sectors is an optimum.
- ❑ Sector geometries:
  - Radial drift
  - Axial drift
  - Azimuthal drift

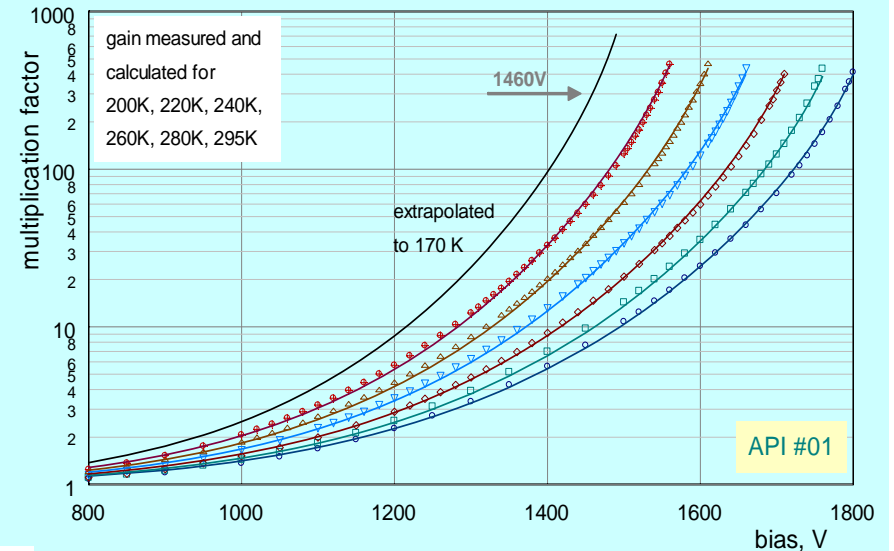
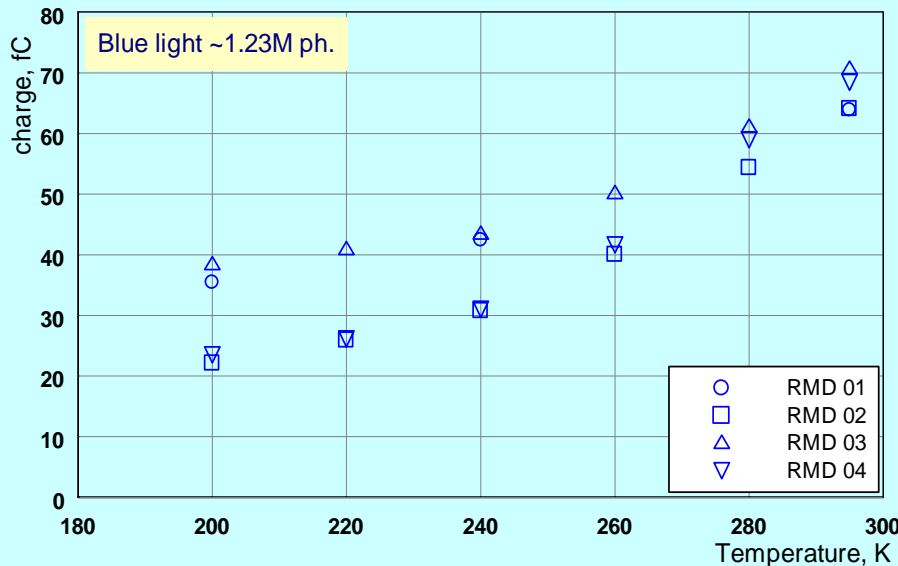
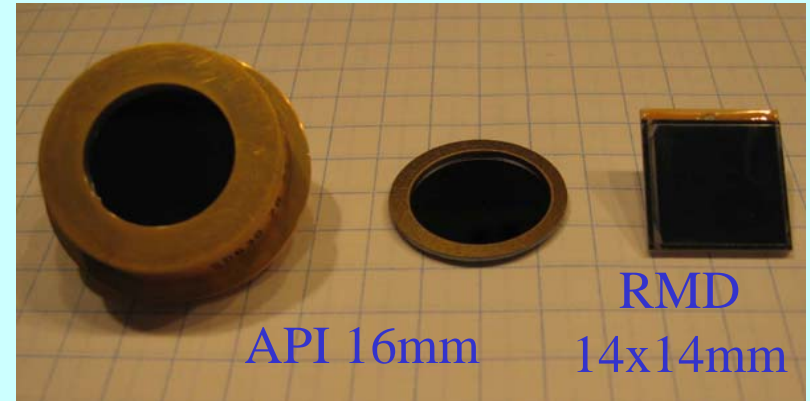


Drift to outer radius has a number of advantages.  
Chosen for prototyping



## Light Detection: APDs

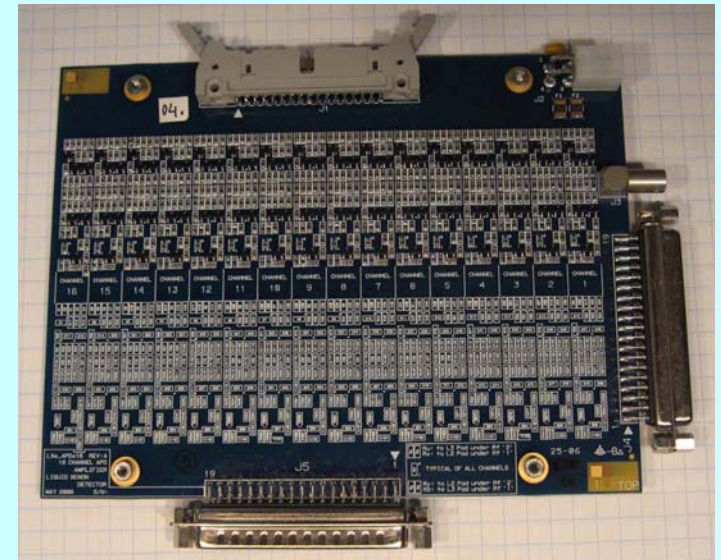
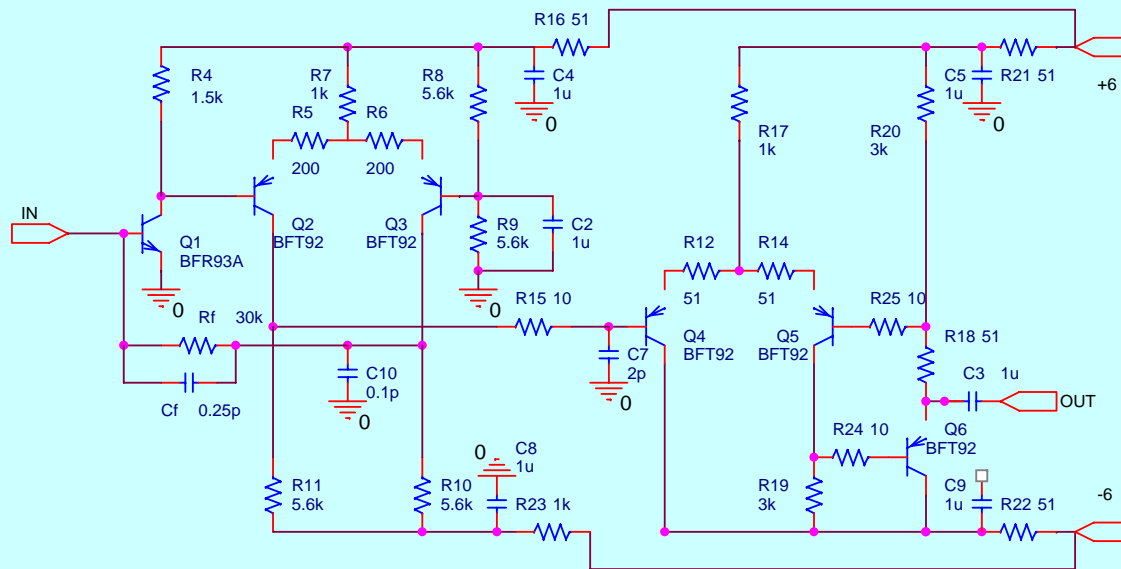
- ❑ PMT: low QE, not compact. Alternative: APD
- ❑ Si works at low T and has  $QE \sim 1$  for UV light. Intrinsically it is fast (few ns)
- ❑ Large area high-gain APDs are available. API and RMD
- ❑ RMD diodes have worse QE at low T





## Light Detection: Electronics

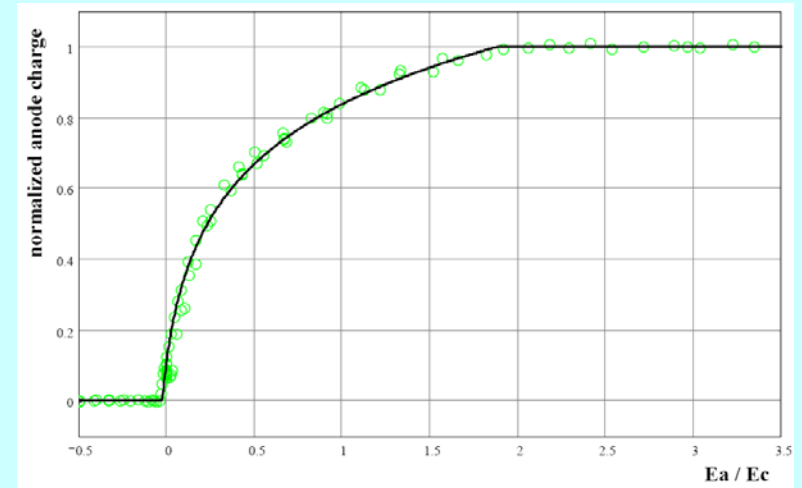
- ❑ Fast and low-noise for  $C_d=200\text{pF}$ , low input impedance
- ❑ For  $2\text{kV/cm}$  and  $SA \cdot QE=0.4\%$  and  $G=500$ ,  $\text{Signal}=20,000e$
- ❑ BJT provides better S/N. ENC  $\sim 4,000e$  for 20 ns peak time
- ❑ Choice of low-noise BJT: Philips BFR93
- ❑ 16-ch prototype done



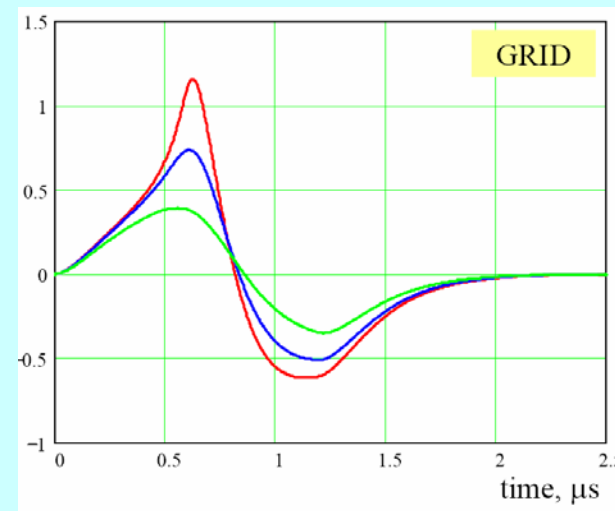
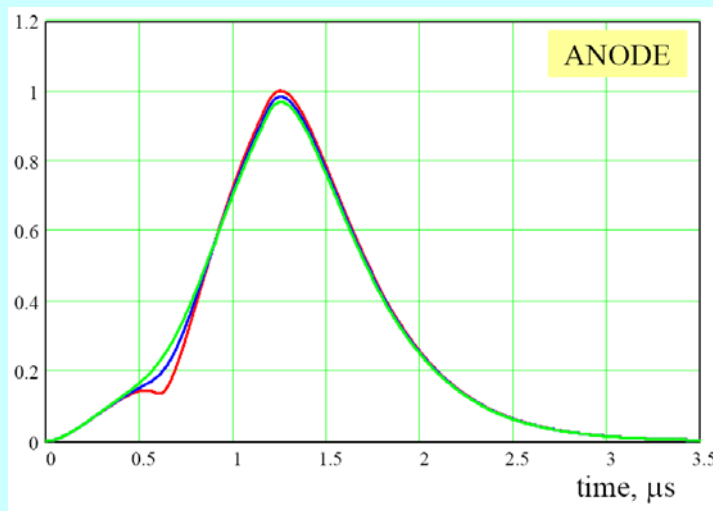


## Charge Measurements

- ❑ Configuration: anode strips (pitch ~1mm), wires (spacing ~1mm), mesh for shielding from drift region. Gaps ~1mm
- ❑ Mesh (SS, cell 500 $\mu\text{m}$ , wire 30 $\mu\text{m}$ ). Transparency measured with gas ionization chamber



- ❑ Induced currents calculated with FEM. Shaper is optimized for S/N

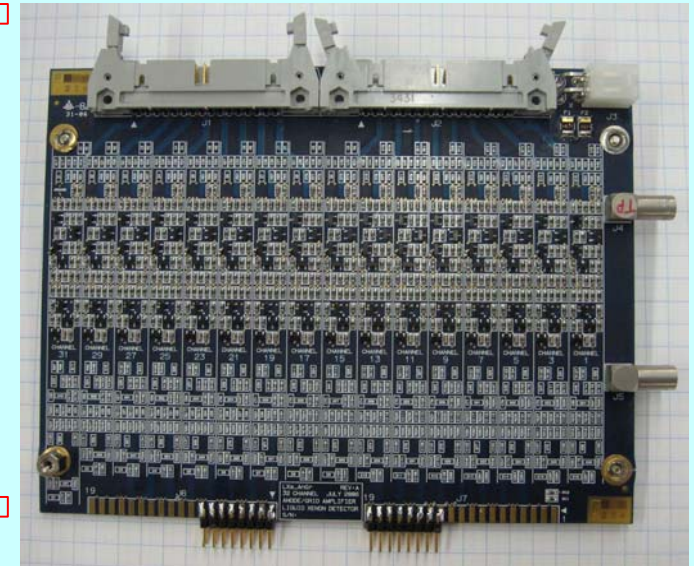
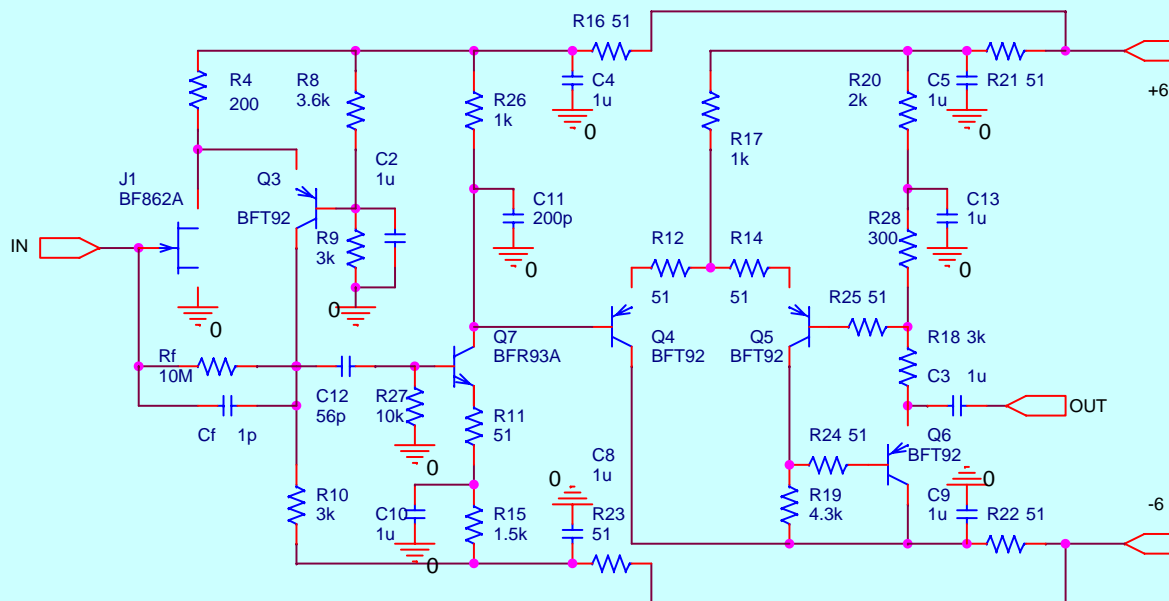






## Electronics for Ionization Signals

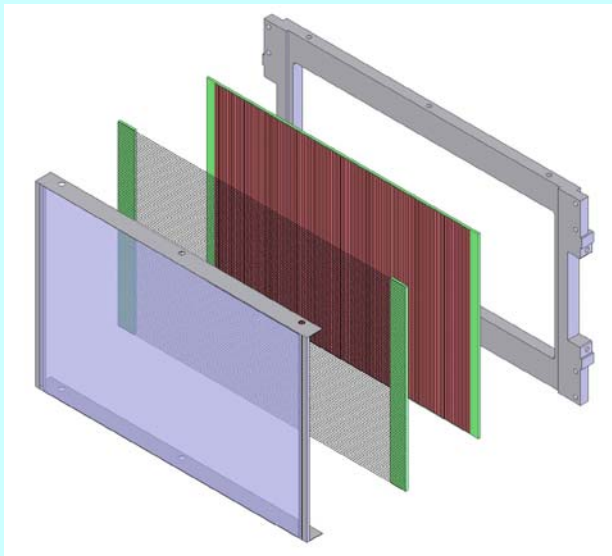
- ❑ Expected signal  $\sim 30,000e$ ; fluctuations  $4\% = 1,200e$
- ❑ Low-noise for  $C_d=20pF$ , and shaping  $\sim 0.3 \mu s$
- ❑ JFET provides better S/N. ENC  $\sim 600e$  for 270ns shaping time
- ❑ Choice of low-noise JFET: Philips BF862
- ❑ 32-ch prototype under tests



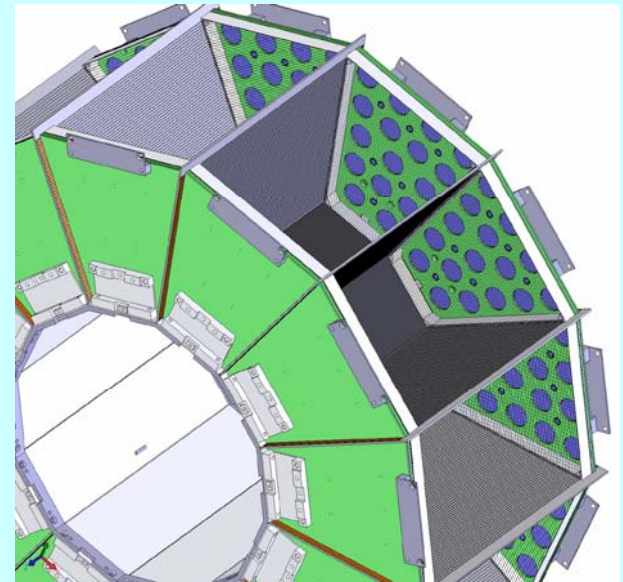


## Full-Scale Prototype

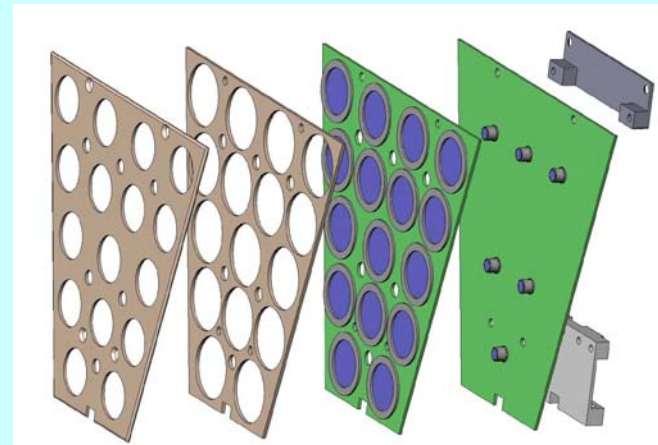
- ❑ 12 sectors.
  - Field cage formed with strips (between sectors) and wires (ends)
  - Cathode: resistive kapton on ceramic plates



- ❑ Anode module
  - 96 wires, 96 strips
  - SS and kapton PCBs
  - AC decoupling with kapton?



- ❑ APD module
  - 16 APDs and 6 LEDs for monitoring
  - 1 HV line and 16 LV lines (HV tuning)

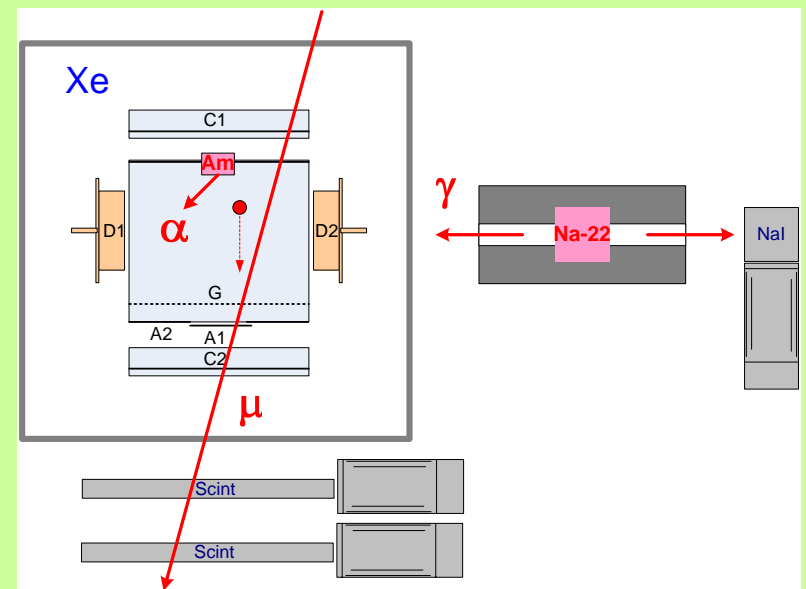
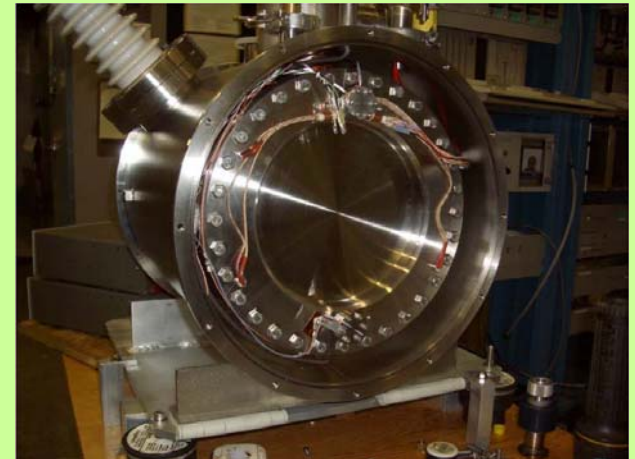






## Small TPC Tests

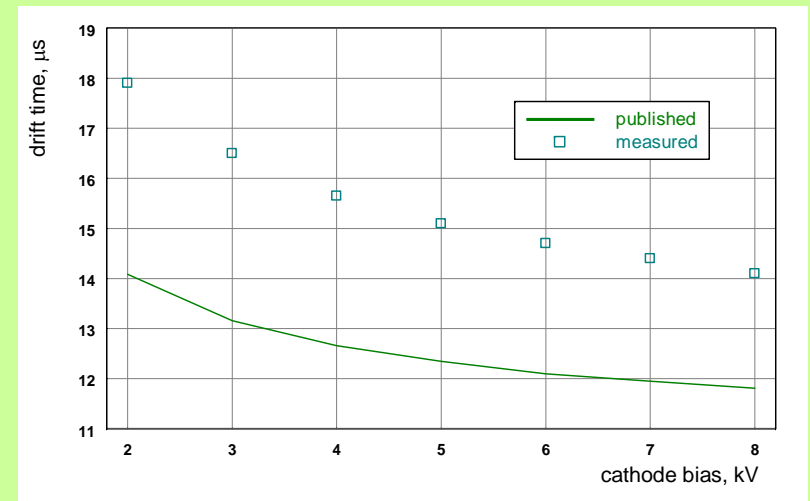
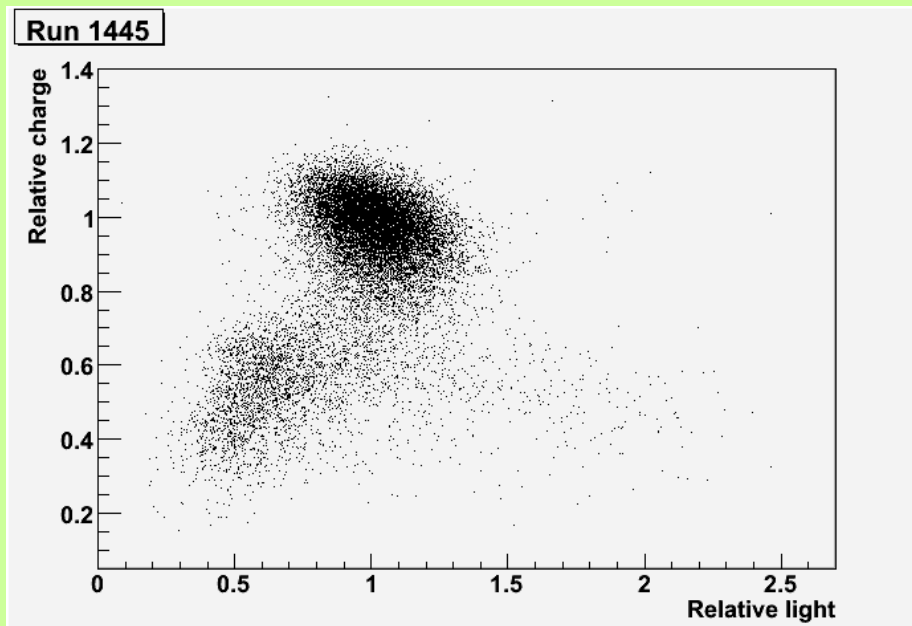
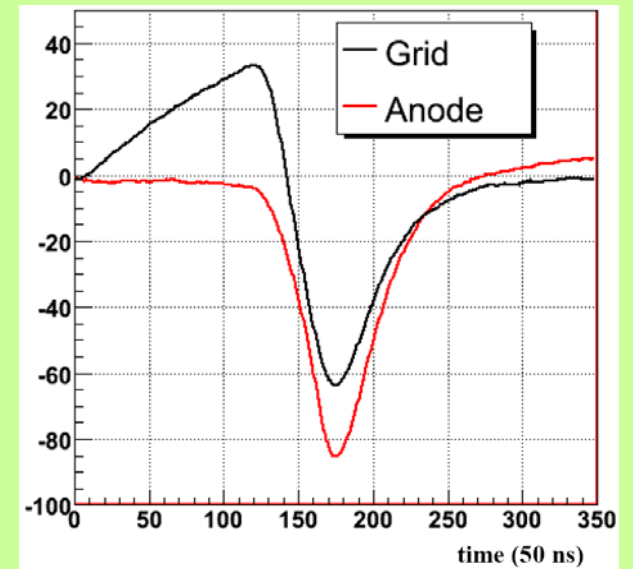
- Run May-August 2006
  - 8.5-l cryostat, small TPC 3x3x3 cm
  - 2 anodes, grid 3 mm gap and 3 mm wire spacing. 2 16mm APDs
  - Both QDC and digitizers
  
- Measured
  - Na-22  $\gamma$  511keV coincidence with external NaI and 1275 keV
  - Cosmic muons
  - Alpha signals
  - Anode and cathode HV curves,
  - APD bias
  - Stability, ...





# Results from Small TPC

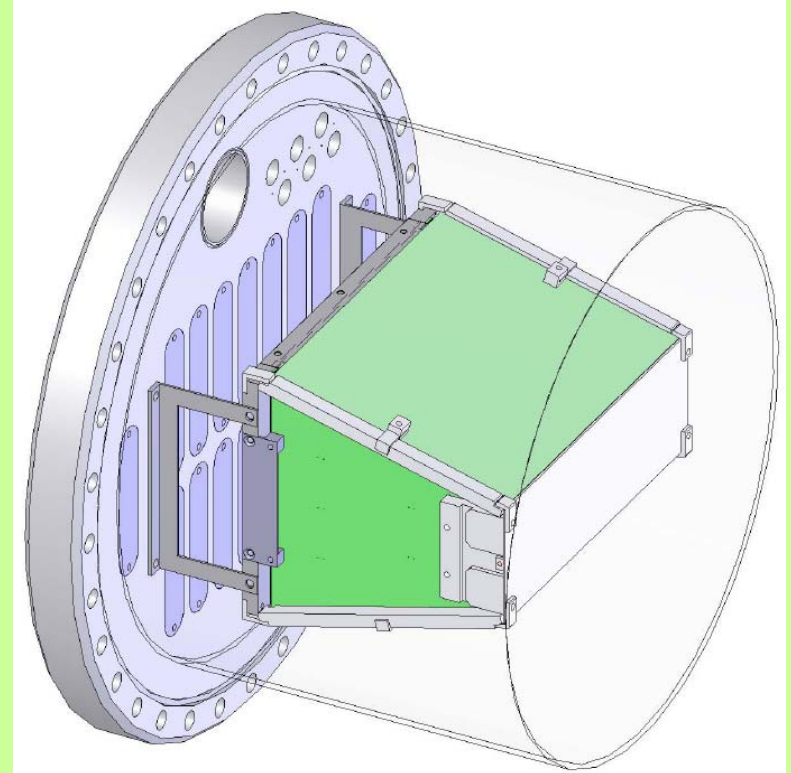
- ❑ Analysis in progress
- ❑ Purity looks OK
- ❑ Ionization signal shapes are reasonable
- ❑ Charge-light anti-correlations are seen
- ❑ Energy resolution (RMS):  
S-12.6%, Q-6.3%, Sum-4.7%





## R&D Program

- ❑ 2006-2007: Sector prototypes
  - Fits to existing cryostat
  - 96 anode strips, 96 grid wires
  - 32 APDs in ends (plus 32 APDs at sides in second prototype)
- ❑ 2007-2008: Two sectors
  - mPET cryostat
  - Final design of sectors
  - Final electronics and readout
- ❑ 2008-2009: PET prototype
  - Fully (half) populated
  - Computing: data farm
  - Develop off-line and image reconstruction SW





## Summary

- ❑ LXe is a very promising technology for PET and other applications
- ❑ Still requires extended R&D to design and build detector
  
- ❑ Supported by CFI-UBC-BCKDF and TRIUMF Tech Transfer Division and Science Division
- ❑ Group:

*P.Amaudruz, D.Bryman, R.Bula, M.Constable, L.Kurchaninov,  
C.Lim, P.Lu, C.Marshall, J.-P.Martin, F. Retiere, T.Ruth,  
V.Semenoff, V.Sossi*